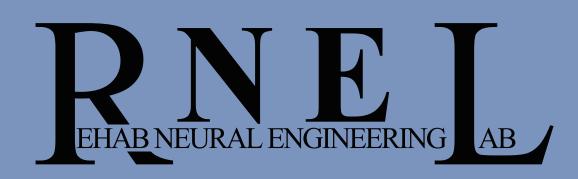
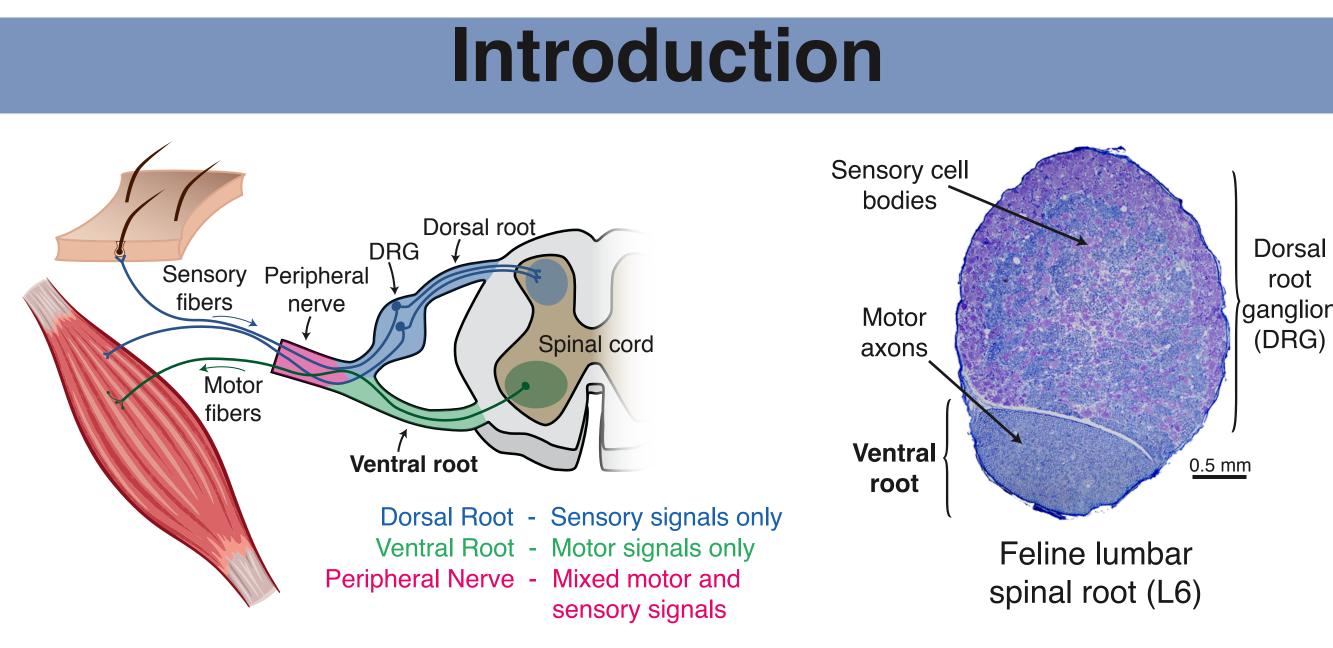
# Estimation of muscle activity from chronic single unit ventral root recordings

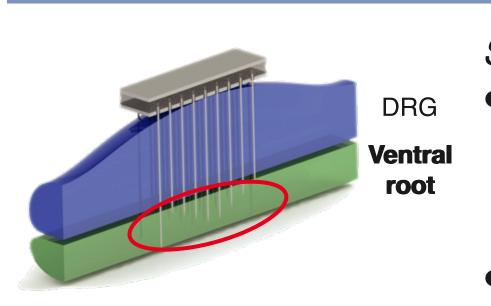


# Matthew J. Bauman<sup>1</sup>, Robert A. Gaunt<sup>1,2</sup>, Douglas J. Weber<sup>1,2,3</sup> Departments of <sup>1</sup>Bioengineering and <sup>2</sup>Physical Medicine & Rehabilitation, University of Pittsburgh, Pittsburgh, PA <sup>3</sup>Department of Veterans Affairs Medical Center, Pittsburgh, PA



- Spinal roots are a promising target for a peripheral neural interface • Motor (ventral) and sensory (dorsal) signals are spatially segregated and
- could be independently targeted for recording and stimulation
- Neural activity in the axons of the ventral root leads directly to muscle contraction and could be used as a source for motor control signals that are directly linked to normal musculoskeletal action
- The spinal column provides more mechanical protection and electrical isolation from muscle activity than is possible in the distal nerves

## **Objective**: Identify and record from motor units in ventral roots and evaluate their ability to estimate muscle activity



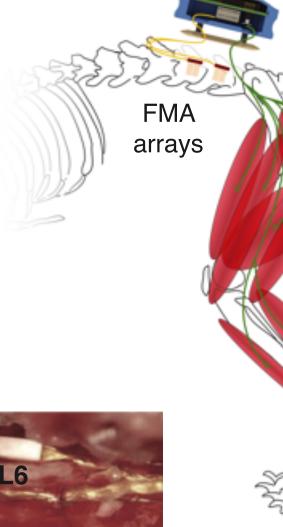
# Methods

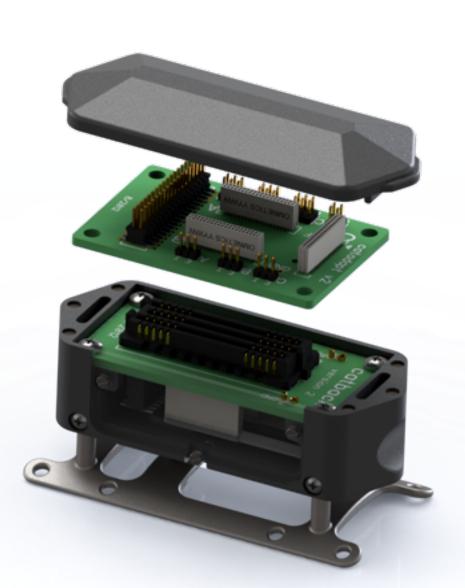
### Sterile surgery

Chronically implanted 32-channel floating microelectrode arrays (FMAs, MicroProbes, Inc.) with varying electrode shank lengths (2.0-3.7mm) in left L6 and L7 spinal nerves of ten adult male cats • Targeted the ventral roots intra-operatively by

until sensory activity was only observed on the shallowest electrodes

- Instrumented up to ten muscles with bipolar intramuscular electromyography (EMG) electrodes
- All signals were routed through custom circuit boards with a single-connector interface (SEARAY, Samtec) mounted within a protective backpack assembly





Experimental procedures

- Neural signals were sampled at 40kHz with a multi-channel neural recording system (DigiAmp, Plexon, Inc) and hand sorted offline, with muscle signals sampled at 20kHz or 40kHz
- Awake (treadmill walking at speeds of 0.4-1.2 m/s) and anesthetized (passive movements, under dexmedetomidine) recording sessions were conducted at least weekly for each cat



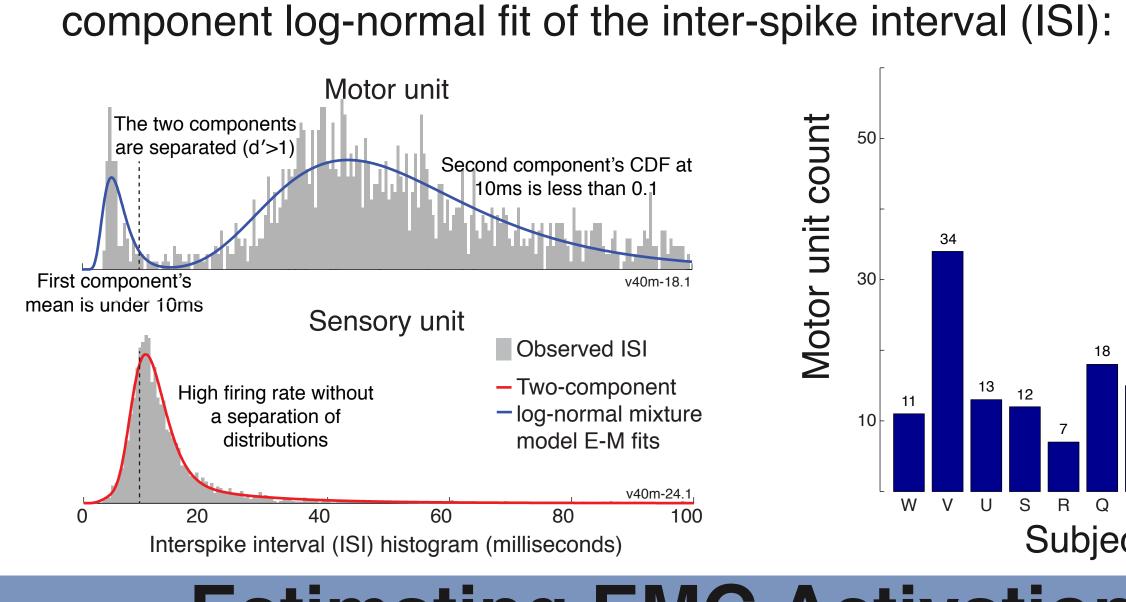
incrementally inserting the array pneumatically

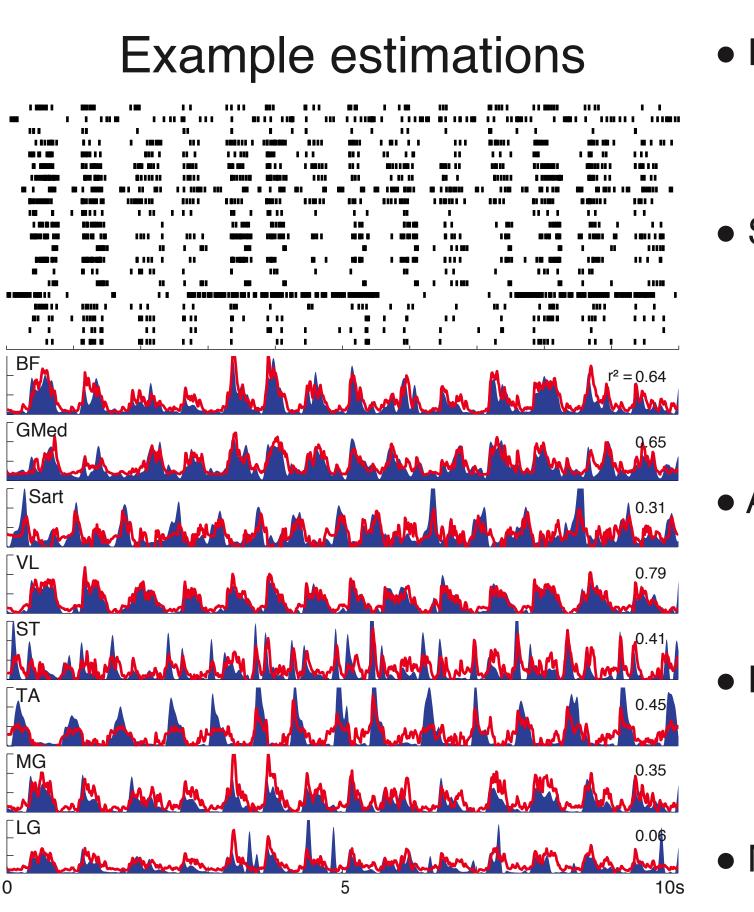
Custom backpack and single-connector nterface for all signals Bipolar

intramuscular EMGs

Units were excluded from analysis if they were: • actively firing during passive movements under anesthesia

- (sensory units will still respond under anesthesia),
- on the same electrode as a unit that was active under anesthesia, • or if they violated 'motor unit-like' firing behavior with a two-



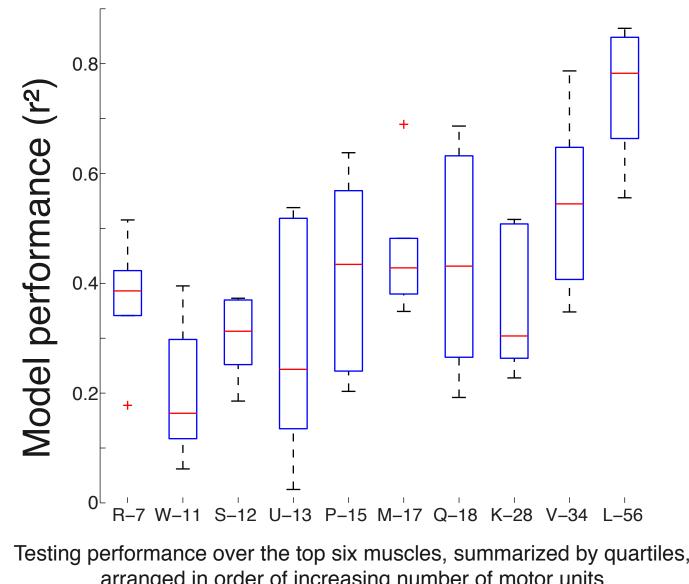


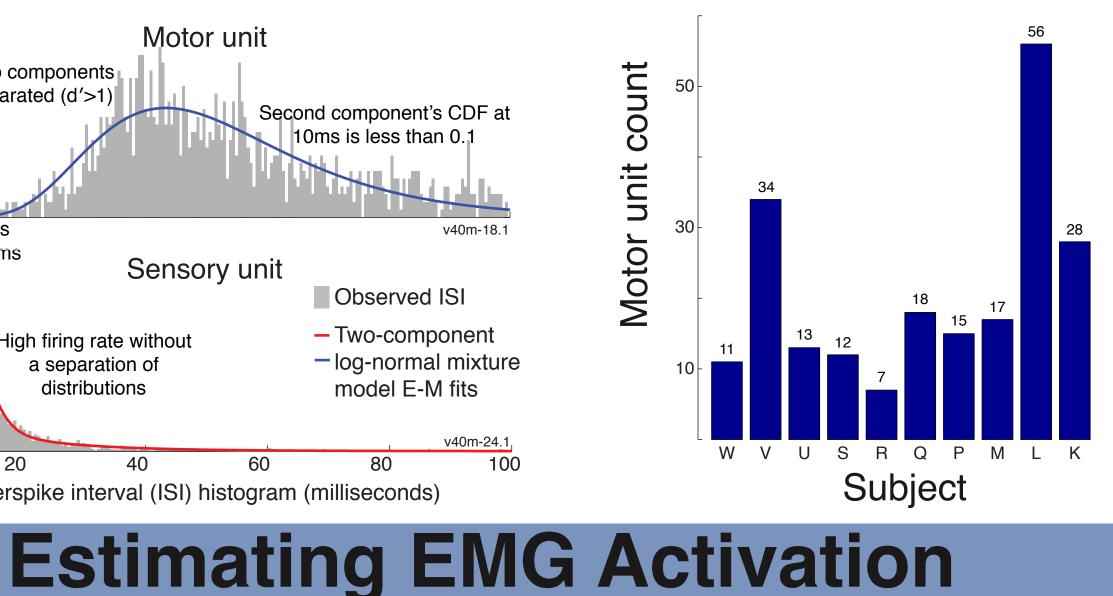
Ten seconds of aligned motor unit (top raster, each row is a unit) and smoothed EMG activity, with the predictions overlaid in red (cat V)

 Models were trained on 50s of treadmill walking data and tested against a later 50s from the same day, with speeds of 0.4-1.2 m/s

## Performance summary

- Four of the subjects have at least three functionally distinct muscles with testing performance  $r^2 > 0.5$
- The number of units is a significant factor (p < 0.01) in the model's r<sup>2</sup> performance, whereas the subject (as a categorical variable) is not significant
- When only considering the highest performing muscle, the number of units is not significant, suggesting only a small number of good units are required for each muscle.





## • EMG Signals were band-pass filtered (50-500Hz), rectified, and smoothed with a low-pass filter (10Hz)

Spikes from units identified as motor units were converted to firing rates (FR) by convolving the spike times with a causal alpha kernel  $a^{2}t \exp(-at)$  with a time constant of 50ms (/ from 0-100ms) • A fitted multiple linear regression models estimated EMG activation from smoothed motor unit firing rates

• Each muscle was considered to be independent, such that:

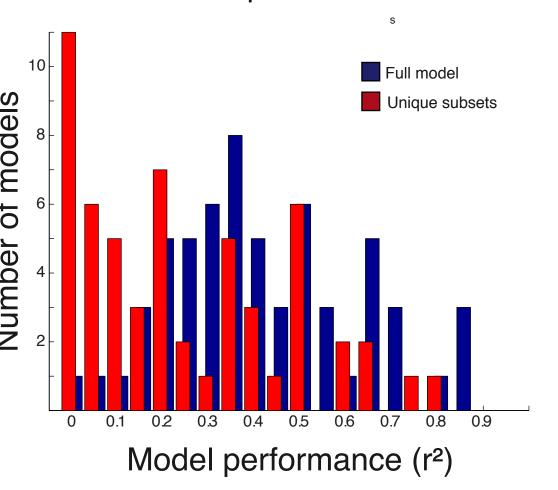
$$EMG_i = b_{i_0} + \sum_j b_{i_j} FR_j$$

arranged in order of increasing number of motor units

# **Physiological Subsetting**

- Each motor unit axon only innervates one muscle, but the multiple linear regression framework uses all units in its estimation of each muscle
- A more physiologically informed approach is to choose a unique subset of motor units to use for each muscle (without replacement)
- Units were selected greedily from the largest significant coefficients of the aggregate models to estimate just one muscle each

Performance compared to full model



- across most of the subjects
- of the recorded units

# Acknowledgements

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- 0.2 Number of units in model
- Some muscles retain very good performance with fewer than three motor unit inputs
- Unlike the aggregate models, there is no significant relationship between number of units and model performance

## **Future Directions**

• Use the known physiology of the motor neuron to refine the regression model, incorporating nonlinearities such as doublets

• We've previously shown that in 29% of our motor unit recordings, we can identify the muscle a motor unit targets through spike-triggered averaging of the evoked muscle potential. Using this information in the subsetted model may improve performance

> • Use the estimated muscle activation to drive input into a musculoskeletal model to predict forces and kinematics

# Summary

• Identified and recorded from motor units in ventral roots

• Estimated EMG activity of all muscles with good performance

• Some muscles were accurately estimated from a very small subset

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